Longitudinal serum S100β and brain aging in the Lothian Birth Cohort 1936

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Elevated serum and cerebrospinal fluid concentrations of S100β, a protein predominantly found in glia, are associated with intracranial injury and neurodegeneration, although concentrations are also influenced by several other factors. The longitudinal association between serum S100β concentrations and brain health in nonpathological aging is unknown. In a large group (baseline N = 593; longitudinal N = 414) of community-dwelling older adults at ages 73 and 76 years, we examined cross-sectional and parallel longitudinal changes between serum S100β and brain MRI parameters: white matter hyperintensities, perivascular space visibility, white matter fractional anisotropy and mean diffusivity (MD), global atrophy, and gray matter volume. Using bivariate change score structural equation models, correcting for age, sex, diabetes, and hypertension, higher S100β concentrations were cross-sectionally associated with poorer general fractional anisotropy (r = −0.155, p = 0.001), which was strongest in the anterior thalamic (r = −0.155, p < 0.001) and cingulum bundles (r = −0.111, p = 0.005), and survived false discovery rate correction. Longitudinally, there were no significant associations between changes in brain imaging parameters and S100β concentrations. These data provide some weak evidence that S100β may be an informative biomarker of brain white matter aging.

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1. Introduction

The calcium-binding protein S100β has clinical value as a proteomic biomarker of central nervous system damage. It is primarily found in glial cells, but also in some neuronal populations and in melanocytes, among other cell types (Donato, 2006; Donato et al., 2013). At nanomolar concentrations, S100β exerts neuroprotective and neurotrophic influences, but elevated S100β may contribute to further negative effects, as its presence at micromolar concentrations increases expression of proinflammatory cytokines, leading to apoptosis (Kleindienst et al., 2010; Rothermundt et al., 2003; Steiner et al., 1999). S100β is elevated after traumatic brain injury in both cerebrospinal fluid (CSF) and serum (Ingebretsen and Romner, 2002; Petzold et al., 2003; Vos et al., 2010), with greater S100β concentrations...
prognostic of poorer outcomes and recovery (Goyal et al., 2013; Thelin et al., 2017). Serum S100β levels are also influenced by blood-brain barrier (BBB) leakage (Kapur et al., 2002; Kleindienst et al., 2010; Ucar et al., 2004), as well as from other sources such as bone fractures, exercise, muscle injury, burns and melanoma (Anderson et al., 2001; Harpio and Einarsson, 2004; Koh and Lee, 2014; Mocellin et al., 2008; Mohammed et al., 2001; Pelinka et al., 2003).

Although S100β has been investigated as a biomarker (in serum and CSF) in studies of head injury, depression, and neurodegenerative diseases such as Alzheimer’s disease (Chaves et al., 2010; Peskind et al., 2001; Polyakova et al., 2015), the serum and CSF concentrations are positively associated with age (Nygaard et al., 1997; Schroeter et al., 2011; van Engelen et al., 1992), although some (Portela et al., 2002; Wiesmann et al., 1998) found no age effect in adulthood. Identifying possible biomarkers of brain aging is a key challenge (Academy of Medical Sciences, 2016; Jylhävä et al., 2017), and serum S100β is one of the logical candidates, yet data on S100β and multimodal brain analyses in older participants are lacking. Two prior cross-sectional studies indicated that serum S100β is specifically associated with poorer white matter microstructure (assessed with diffusion tensor MRI) in a small sample of healthy participants (N = 41, effect found in females only; Streitburger et al., 2012), and in a small study of schizophrenia patients versus controls (total N = 39; Milleit et al., 2016). Neither study found a significant association between S100β and gray matter (GM)—however, it should be noted that both adopted a voxel-based-morphometry approach which results in reduced power in the large areas of the cortex that show highly individualized patterns of gyrification, and insensitivity to discrete lesions; Tisserand et al., 2004). Another study (N = 102; van der Leeuw et al., 2017) found no association between S100β and either white matter fractional anisotropy (FA) or cortical thickness in a mixed sample of patients with psychosis, relatives, and controls. Thus, well-powered, longitudinal, multimodal imaging studies—in participants at an age that confers relatively high risk of brain structural decline—are required to examine the possible differential sensitivity of S100β to cross-sectional levels of, and longitudinal declines in, various imaging parameters and brain tissues.

Other candidate MRI parameters that may relate to S100β are markers of cerebral small vessel disease (SVD) burden. There is increasing evidence that BBB leakage occurs as an underlying mechanism of plasma S100β concentration in blood may rise due to age, central nervous system (CNS) damage, and BBB disruption, we hypothesized that relatively higher and increasing concentrations of plasma S100β would be coupled with lower and decreasing measures of brain structural and microstructural health. Prior evidence indicates that S100β is particularly strongly expressed in the human brain’s white matter tracts (histological data showed co-localization of S100β with oligodendrocyte markers in the human brain; Streitburger et al., 2012), and that serum S100β is cross-sectionally associated with poorer white matter microstructure (assessed with diffusion tensor MRI) in small mixed samples (N ≤ 102) with wide age ranges (Milleit et al., 2016; Streitburger et al., 2012). Thus, we hypothesize that elevated and increasing serum S100β would be particularly pertinent to poorer and decreasing white matter structure, beyond measures of global atrophy and GM volume.

2. Materials and methods

2.1. Participants

Data are drawn from waves 2 and 3 of a longitudinal study of aging: the Lothian Birth Cohort 1936 study (LBC1936; Deary et al., 2007; 2012), when participants were a mean age of about 73 and 76 years, respectively. In 1947, Scotland tested the intelligence of almost all schoolchildren born in 1936, and the LBC1936 follows up some of those individuals—now in older age—who mostly live in the Edinburgh and Lothians area. The initial wave of LBC1936 (wave 1) took place between 2004 and 2007. It assessed 1091 individuals on aspects of their health, and physical and cognitive function, at around 70 years old (M = 69.53, SD = 0.832). At wave 2 (2007–2011) and wave 3 (2011–2013), 866 and 697, respectively, returned at mean ages of about 73 and 76 years, a detailed MRI brain scan was added to the protocol at both waves (Wardlaw et al., 2011). During a medical interview at each wave, participants reported their medical history (including a self-reported diagnosis of hypertension, diabetes, melanoma, and dementia). The Multi-Centre Research Ethics Committee for Scotland (MREC/01/0/56), the Scotland A Research Ethics Committee (07/MRE00/58), and the Lothian Research Ethics Committee (LREC/2003/2/29) approved the use of the human participants in this study; all participants provided written informed consent and these have been kept on file.

2.2. S100β

Serum samples were obtained from participants during the main physical and cognitive testing appointment at waves 2 and 3. The mean lag between waves was 3.77 years (SD = 0.28). After collection, samples were stored at –80 °C at the Wellcome Trust Clinical Research Facility, Western General Hospital, Edinburgh, until the conclusion of the wave. They were then transferred to the Department of Clinical Biochemistry, King’s College London using cold-chain logistics, where they were stored at −20 °C rather than –80 °C was an average of 44 days (SD = 26) for 4 batches at wave 2, and 8 days (single batch) at wave 3, respectively. The minimal detectable concentration of the assay was 0.02 μg/L. Intra- and inter-assay precision for both waves is reported in Supplementary Table A1.
2.3. MRI acquisition and processing

Participants underwent whole-brain structural and diffusion MRI using the same 1.5 T GE Signa Horizon scanner (General Electric, Milwaukee, WI, USA) at wave 2 and 3. The scanner was maintained with a careful quality control programme. Scans took place at the Brain Research Imaging Centre, Edinburgh, shortly after serum collection (mean lag for the present study sample: wave 2 M = 65.39 days, SD = 34.69; wave 3 M = 38.69 days, SD = 28.37). Full details of acquisition and processing are available in an open access protocol article (Wardlaw et al., 2011). Briefly, T₁-w, T₂-w, T₂*-w, and FLAIR-weighted sequences were co-registered (voxel size = 1 × 1 × 2 mm). Total brain (TB), GM, and white matter hyperintensity volumes were quantified using a semiautomated multispectral fusion method (Valdés Hernández et al., 2010). WMHs were explicitly defined as punctate, focal, or diffuse lesions in subcortical regions and distinguished from lacunes and PVS by signal characteristics (Wardlaw et al., 2012). Cortical or discrete subcortical infarcts were excluded by careful manual editing blind to other features. PVS were defined as fluid-containing small spaces running parallel with the expected direction of perforating vessels, appearing punctate in cross section and linear in longitudinal section, with <3 mm diameter. PVS were differentiated from lacunes or WMH on morphology, and size criteria as previously defined (Wardlaw et al., 2013; Potter et al., 2015a). From the T₂-weighted volumes, PVS ratings were performed by a trained neuroradiologist (JM.W, Z.M; Potter et al., 2015a; Potter et al., 2015b). Change in PVS between waves was scored by comparing scans at wave 2 and wave 3 side by side, blind to any other participant characteristics, and scored on a 5-point scale from −2 (reduction, i.e., improvement) to +2 (increase, i.e., worsening), where 0 denotes no visible change.

The diffusion tensor MRI (DT-MRI) acquisition comprised a single-shot spin-echo echo-planar diffusion weighted volumes (b = 1000 s mm⁻²) acquired in 64 noncollinear directions, alongside 7 T₂-weighted images (b = 0 s mm⁻²). This yielded 72 contiguous axial slices (FoV = 256 × 256 mm, matrix 128 × 128, 2 mm isotropic voxels). Repetition and echo times were 16.5 s and 95.5 ms, respectively. After preprocessing (brain extraction, removal of bulk participant motion and eddy current distortions), water diffusion tensor parameters were estimated using FSL tools (FMRIB; Oxford, UK; http://www.fmrib.ox.ac.uk). A 2-fiber model with 5000 streamlines was then used to create brain connectivity data using the BEDPOSTX/ProbTractKx algorithm in 12 tracts of interest: the genu and splenium of the corpus callosus, bilateral anterior thalamic radiation, cingulum, uncinate, arcuate, and inferior longitudinal fasciculi. Probabilistic neighborhood tractography as implemented in the TractoR package (http://www.tractor-mri.org.uk; Clayden et al., 2011) identified the tracts of interest from the connectivity data (Bastin et al., 2010; Munoz Maniega et al., 2017). White matter tract-averaged FA and mean diffusivity (MD) were then derived as the average of all voxels contained within the resultant tract maps. All segmented images were visually inspected for accuracy, blind to participant characteristics, to identify and correct errors.

2.4. Statistical analysis

We excluded from the analyses those with self-reported history of dementia, or Mini-Mental State Examination score of <24 (n = 35). This was based on prior reports of elevated S100β in dementia (Chaves et al., 2010), the likelihood that these individuals were undergoing pathological CNS degeneration, and their low numbers in the current cohort (yielding low statistical power with which to reliably detect associations). Given that elevated serum S100β is associated with melanoma (Harpio and Einarsson, 2004; Mocellin et al., 2008; Mohammed et al., 2001), those who reported melanoma at either wave (n = 26) were also excluded. S100β concentrations for excluded participants are shown in Supplementary Table A.2. Both WMH measures were log transformed to correct skewness. Extreme outlying points (>4 SDs above the mean) for S100β at wave 2 (n = 6) and wave 3 (n = 4) were removed, along with 7 points at wave 3 that were below the sensitivity threshold of the assay (<0.02 μg/L). After exclusions, a total of 776 and 619 participants provided S100β data at ages 73 and 76 years, respectively, 593 and 414 of whom also provided brain MRI data. We used the maximum available sample size in all analyses.

The main questions we addressed were (1) are there associations between serum S100β and brain imaging variables cross-sectionally at age 73 years? and (2) are the changes in S100β from age 73 years to age 76 years correlated with changes in brain imaging variables across the same ages? We used bivariate change score models (McArdle, 2009) in a structural equation modeling (SEM) framework to test these cross-sectional and longitudinal associations between S100β and brain MRI variables (Fig. 1), specifying a separate model for each brain MRI outcome. In the case of PVS analysis, the visual rating of PVS change was used in place of a latent change score, and correlated with the latent S100β change score. The volumetric brain indices were expressed as a proportion of intracranial volume in our main SEMs, and we also provided a supplementary analysis for uncorrected measures. Using the FA and MD measures across multiple white matter tracts, we derived a latent variable (hereafter referred to as gFA and gMD) for waves 2 and 3, respectively, using the following: genu and splenium of the corpus callosus, and left-right averages of the anterior thalamic radiation, inferior longitudinal fasciculus, uncinate, arcuate, and cingulum. We imposed strict factorial invariance (as was previously shown to be possible for these data; Ritchie et al., 2015), constraining the intercepts of each tract measure and their loadings on the latent variable to equality across waves. We also included correlated residuals between corresponding tracts across waves, alongside 5 other significant tract-tract residual paths for gFA and gMD. This builds on our and others’ prior work, which found that there is substantial shared variance in white matter microstructural properties across tracts of the brain in early life, middle, and older age (Cox et al., 2016; Penke et al., 2010; Ritchie et al., 2015; Telford et al., 2017). Thus, these general, latent, factors reflect common microstructural properties (FA and MD) across white matter pathways. Finally, based on evidence of local white matter variation in S100β expression (most strongly expressed in the corpus callosus and cingulum bundle) and cross-sectional associations between FA and S100β (Streitbürger et al., 2012; Milleit et al., 2016; van der Leeuw et al., 2017; Allen Institute for Brain Science, 2010), we used the same framework as above to examine associations between S100β and tract-specific microstructure in each white matter tract of interest for FA and MD.

Given that there was a short delay between serum collection and MRI scanning at both waves, we corrected MRI and S100β for their respective age in days at data collection within each model, along with sex, diabetes, and hypertension. To account for missing data bias due to attrition between waves, we took account of all available data, using full information maximum likelihood estimation. We assessed model fit according to the χ² minimum function test statistic, the root mean square error of approximation (RMSEA), comparative fit index (CFI), Tucker-Lewis index (TLI), and the standardized root mean square residual (SRMR). All statistical analyses were conducted in R version 3.2.2 “Fire Safety” (R Core Team, 2015). SEM was conducted with the “lavaan” package (Rosseel,
2012) and the resultant p-values for the associations of interest (see asterisks in Fig. 1) were corrected for multiple comparisons with false discovery rate (FDR; Benjamini and Hochberg, 1995) using the "p.adjust" function in R.

3. Results

3.1. Participant and S100β descriptives, and analysis of losses to follow-up

Participant characteristics are shown in Table 1, and bivariate associations among study variables are reported in Supplementary Table A3. Descriptive plots of S100β (density, and age 73–76 years correlation, boxplot, and trajectory) are in Fig. 2. S100β concentrations showed substantial stability of individual differences from age 73 years to age 76 years (Pearson’s r = 0.585, p < 0.001). S100β concentrations were significantly higher at age 76 years than at age 73 years (when considering returners only: wave 2 S100β M = 0.085, SD = 0.035; wave 3 S100β M = 0.092, SD = 0.040; t (1190.70) = 3.244, p = 0.001, Cohen’s d = 0.118). Males showed lower S100β than females at both waves (wave 2: t (773.28) = 3.655, p < 0.001; wave 3: t (614.69), p = 0.002), but did not exhibit differences in their rate of change with age (p = 0.546; Fig. 2).

When comparing baseline values of those who returned to provide an S100β sample at age 76 years from those who did not, there were no significant differences for S100β (t (270.19) = 0.115, p = 0.908), TB volume (t (167.74) = 1.577, p = 0.117), WMH volume (t (152.70) = 1.277, p = 0.204). However, individuals who returned at age 76 years had significantly more GM at age 73 years than nonreturners (t (174.00) = 2.800, p = 0.006). To satisfy the assumption of missing at random (MAR; Rubin, 1976), under which FIML operates, baseline GM volume was included as an auxiliary variable (Schafer and Graham, 2002) when modeling associations between S100β and all other imaging variables. Significant increases in WMH volume and white matter tract MD, and significant decreases in TB volume, GM volume, and white matter FA exhibited by this cohort between wave 2 and 3 have been previously reported elsewhere (Dickie et al., 2016; Ritchie et al., 2015). In the context of the current sample, all brain measures showed statistically significant mean changes over time, considering only those who provided scans at both waves. There were significant reductions in raw TB (t (851.73) = 2.815, p = 0.005, Cohen’s d = 0.191) and GM volume (t (844.37) = 2.861, p = 0.004, Cohen’s d = 0.197), and increases in WMH volumes (t (809.50) = 4.267, p < 0.001, Cohen’s d = 0.293). The visual ratings of PVS change across waves showed that PVS load was worse over time (N = 426 received a score of 0) or became worse over time (N = 42 received a score of +1). Those who provided S100β and did not undergo an MRI scan were not significantly different from those who provided both—at either wave 2 or wave 3—in terms of age, S100β concentrations, and Mini-Mental State

![Fig. 1. Example of bivariate change score models. Baseline level of, and 3-year change in, S100β is associated with the wave 2 level and wave 2–wave 3 (age 73–76 years) change in (A) a latent factorially invariant measure of FA, and (B) white matter hyperintensity volume. Individual tract-averaged values in (A) are A:G (correlated residuals not shown). For PVS, to the Web version of this article.)](image-url)

### Table 1: Participant characteristics

<table>
<thead>
<tr>
<th>Variable</th>
<th>Units</th>
<th>Wave 2 (age 73 y)</th>
<th>Wave 3 (age 76 y)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Mean (SD)</td>
<td>N</td>
<td>Mean (SD)</td>
</tr>
<tr>
<td>Sex</td>
<td>M:F</td>
<td>395.381</td>
<td>776</td>
</tr>
<tr>
<td>Age S100β</td>
<td>Years</td>
<td>72.493 (0.716)</td>
<td>776</td>
</tr>
<tr>
<td>S100β</td>
<td>µg/L</td>
<td>0.085 (0.035)</td>
<td>776</td>
</tr>
<tr>
<td>MMSE</td>
<td>(30)</td>
<td>28.815 (1.285)</td>
<td>775</td>
</tr>
<tr>
<td>WMH</td>
<td>cm³</td>
<td>8.060 (11.376)*</td>
<td>592</td>
</tr>
<tr>
<td>Total Brain</td>
<td>cm³</td>
<td>991.176 (90.522)</td>
<td>593</td>
</tr>
<tr>
<td>GM</td>
<td>cm³</td>
<td>472.862 (44.860)</td>
<td>593</td>
</tr>
</tbody>
</table>

Descriptive MRI data are provided for those that gave S100β at the same wave. Key: GM, gray matter volume; MMSE, Mini-Mental State Examination; WMH, white matter hyperintensity volume (untransformed).

* Median and IQR provided for raw (untransformed) volumes.
Examination score (all t values < 0.779, p > 0.437). However, those who undertook both elements of the study comprised a significantly larger proportion of males at wave 2 (χ² = 5.708, p = 0.017), although not at wave 3 (χ² = 2.303, p = 0.129).

3.2. Cross-sectional and longitudinal associations between S100β and global MRI

Individuals showed substantial variation in the degree to which S100β and the continuous MRI indices changed over time, as indicated by significant slope variances (all p < 0.001); slope means and variances from age- and sex-corrected univariate change score models are reported in Supplementary Table A.4. Results of the SEM analyses are shown in Table 2, with bias-corrected 95% confidence intervals from 1000 bootstraps. Model fit statistics are shown in Supplementary Table A.5. Models examining associations between the level and change of S100β and volumetric MRI indices showed adequate fit to the data (WMH: χ²(28) = 42.629, RMSEA = 0.023, CFI = 0.993, TLI = 0.988, SRMR = 0.026; GM: χ²(24) = 42.337, RMSEA = 0.027, CFI = 0.987, TLI = 0.977, SRMR = 0.022; TB volume: χ²(28) = 131.237, RMSEA = 0.060, CFI = 0.931, TLI = 0.887, SRMR = 0.039). None of these measures showed significant cross-sectional associations with S100β at age 73 years (all absolute r-values ≤ 0.061, all p-values ≥ 0.113) or longitudinally (all absolute r-values ≤ 0.082, all p-values ≥ 0.095). Running these volumetric analyses without correction for intracranial volume did not substantially alter the results (Supplementary Table A.6). The model of visually rated PVS change showed an adequate fit to the data (χ²(14) = 39.439, RMSEA = 0.042, CFI = 0.963, TLI = 0.936, SRMR = 0.032). There was no association between S100β at age 73 years and visually rated PVS change (r = −0.034, p = 0.475), and the nominally significant association with longitudinal S100β concentrations (r = −0.096, p = 0.041) did not survive FDR correction.

The models examining associations of S100β with white matter diffusion parameters both fitted the data well (gFA: χ²(205) = 284.004, RMSEA = 0.019, CFI = 0.977, TLI = 0.969, SRMR = 0.035 and gMD: χ²(205) = 322.817, RMSEA = 0.024, CFI = 0.970, TLI = 0.959, SRMR = 0.048); tract loadings are reported in Supplementary Table A.7. At wave 2, higher S100β was significantly associated with “less healthy” white matter gFA (i.e., poorer directional coherence of water molecular diffusion; r = −0.150, p = 0.001), which survived correction for multiple comparisons. The 3-year association between declining gFA and increasing S100β was nonsignificant (r = −0.083, p = 0.154). Associations between gMD...
and S100β were nonsignificant for both level ($r = 0.003, p = 0.941$) and change ($r = 0.019, p = 0.717$).

### 3.3. Cross-sectional and longitudinal associations between S100β and white matter tract-specific microstructure

Next, we examined the level and change associations between S100β and average white matter microstructure (FA and MD) within each of the tracts of interest. Fit statistics indicated that all models fitted the data well (Supplementary Tables A.8 and A.9). Results of the models are shown in Fig. 3, and Supplementary Tables A.10 and A.11. A higher concentration of S100β at age 73 years was significantly associated with “poorer” FA at the same age in the anterior thalamic radiation ($r = -0.155, p < 0.001$) and cingulum bundle ($r = -0.111, p = 0.005$). Both survived FDR correction. There were also nominally significant associations with the level of the splenium ($r = -0.087, p = 0.030$) and arcuate ($r = -0.087, p = 0.032$) in the same direction, but these did not survive multiple comparison correction. The corresponding associations for tract MD were all nonsignificant cross-sectionally (all absolute $r$ values $\leq 0.059$ $p$-values $\geq 0.138$) and longitudinally (all absolute $r$ values $\leq 0.069$ $p$-values $\geq 0.158$).

### 4. Discussion

These data represent the first large-scale study of longitudinal S100β concentrations and their association with longitudinal multimodal brain vascular and neurodegeneration MRI markers in community-dwelling older adults. We focused on multiple MRI indices of brain white matter because S100β is predominantly found in glial cells. We also considered measures of GM and global atrophy as comparators. Notably, our results suggest that individual differences in serum S100β concentrations may be potentially informative for specific aspects of brain white matter aging. We found that higher S100β was, in cross-sectional analysis at age 73 years, significantly associated with generally poorer white matter microstructure (as indexed by gFA), with a small effect size (Cohen, 1992). Further investigation of tract-specific effects indicated that this association is predominantly driven by lower FA in the anterior thalamic, arcuate, cingulum, and callosal fibers.

The significant gFA-S100β association at age 73 years reported here contradicts some (van der Leeuw et al., 2017) but corroborates other (Milleit et al., 2016; Streitbürger et al., 2012) previous cross-sectional associations in smaller ($N \leq 102$) samples. Our well-powered longitudinal design provides important new data on the coevolution of this serum biomarker with brain MRI, including several measures that had not previously been examined, such as white matter MD and markers of SVD. Given the prevalent不明白

<table>
<thead>
<tr>
<th>Variable</th>
<th>Cross-sectional (age 73 y)</th>
<th>95% CI</th>
<th>Longitudinal (age 73–76 y)</th>
<th>95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Lower</td>
<td>Upper</td>
<td>Lower</td>
<td>Upper</td>
</tr>
<tr>
<td>WMH^a</td>
<td>-0.019 (0.634)</td>
<td>-0.092</td>
<td>0.074</td>
<td>0.082 (0.095)</td>
</tr>
<tr>
<td>PVS</td>
<td>-0.034 (0.475)^a</td>
<td>-0.132</td>
<td>0.050</td>
<td>-0.096 (0.041)^a</td>
</tr>
<tr>
<td>gFA</td>
<td>-0.150 (0.001)</td>
<td>-0.233</td>
<td>-0.065</td>
<td>-0.083 (0.154)</td>
</tr>
<tr>
<td>gMD</td>
<td>0.003 (0.941)</td>
<td>-0.099</td>
<td>0.114</td>
<td>-0.019 (0.717)</td>
</tr>
<tr>
<td>GM</td>
<td>0.061 (0.133)</td>
<td>-0.021</td>
<td>0.127</td>
<td>-0.050 (0.309)</td>
</tr>
<tr>
<td>TBV</td>
<td>0.045 (0.272)</td>
<td>-0.024</td>
<td>0.125</td>
<td>-0.044 (0.364)</td>
</tr>
</tbody>
</table>

Data are shown as standardized coefficients ($p$-values), with bootstrapped 95% confidence intervals (CIs) from 1000 draws. Bold text indicates FDR $q < 0.05$.

Key: FDR, false discovery rate; gFA, general factor of white matter tract fractional anisotropy; gMD, general factor of white matter tract mean diffusivity; GM, gray matter volume; PVS, perivascular space rating; TBV, total brain volume; WMH, white matter hyperintensity volume.

^a coefficients are for associations between visually rated PVS change (rather than a latent change score) with S100β level and change.

Fig. 3. Cross-sectional and longitudinal associations between S100β and white matter tract microstructure. Left panel shows superior and lateral views of tracts of interest (with WMH for illustration) using MRI data from a single LC1936 participant. Right panel indicates the association magnitude ($r$) for S100β-tract (FA and MD) associations at baseline (cross-sectional at age 73 years; dark blue and dark green) and coupled 3 years change (longitudinal changes in S100β and microstructure from age 73 to 76 years; light blue and light green), with standard error bars. Black and red asterisks denote nominal ($p < 0.05$) and FDR-corrected significance, respectively. Estimates and $p$-values are reported in Supplementary Tables A.8 and A.9. Abbreviations: FA, fractional anisotropy; FDR, false discovery rate; MD, mean diffusivity; WMH, white matter hyperintensity. (For interpretation of the references to color in this figure legend, the reader is referred to the Web version of this article.)
our findings that higher concentrations are related to poorer white matter FA could partly be related to deleterious effects due to systemic inflammation. Systemic inflammatory challenge reportedly elicits increased BBB permeability in humans and rodent models (Elwood et al., 2017), and there are relationships between higher inflammatory markers and lower brain metrics, including white matter markers of SVD (Arribasal et al., 2014; Corlier et al., 2018, reviewed in; Persson et al., 2014 and in; Wardlaw et al., 2013). Consequently, it will be of interest to quantify the degree to which the relationship between inflammation and cognitive decline is mediated by $\beta$S100 and brain structural outcomes, as well as to identify the potential genetic and lifestyle determinants of inflammation (e.g., Corlier et al., 2018) in well-powered longitudinal designs. Taken together, our results provide some limited support for the hypothesis that both (serum markers and brain MRI) provide meaningful and overlapping biomarkers of age-related white matter degradation.

This study also provides novel information about the concentrations and stability of individual differences in serum $\beta$S100 (i.e., the correlation between samples taken 3 years apart), in generally healthy older adults. These may suggest that serum $\beta$S100 concentrations in the same individual may represent a relatively stable trait, although establishing this more robustly would require many more sampling occasions. We also provide information on sex differences in the context of important confounds of age, melanoma, dementia, sleep apnea, depression, time of year/season, bone fractures, muscle injury, and burns (Anderson et al., 2001; Chaves et al., 2010; Harpio and Einarsson, 2004; Koh and Lee, 2014; Mohammed et al., 2001; Morera-Fumero et al., 2013; Pelinka et al., 2003; Peskind et al., 2001; Polyakova et al., 2015; Traxdorf et al., 2016), only some of which (dementia and melanoma) were accounted for in the present analyses. Our measure of PVS and its change is likely to be relatively insensitive; the rater could not be blinded to time, and the binary and disproportionate nature of visually rated PVS change mean that the estimates reported here should be interpreted accordingly. Computational methods for PVS quantification that are currently in development (Ballerini et al., 2016) may improve sensitivity to detect important aging-related changes. Finally, the narrow age range, ethnic homogeneity (all participants were White British), and relative good health of study participants limits the degree to which our findings can be generalized to groups of different ages, ethnicities, and patients. Nevertheless, the fact that these characteristics obviate such strong potential confounds in the current analysis can be viewed as an important strength.

Combined with the large sample size, longitudinal data, rich multimodal imaging parameters, same-scanner MRI acquisition, advanced and appropriate statistical modeling, and inclusion of important covariates, the present study is well-suited to test hypotheses about cross-sectional and short-term longitudinal associations between serum $\beta$S100 and brain structural aging. High and increasing concentrations of serum $\beta$S100 at this age are identified here as a potentially meaningful marker of poorer brain white matter health and, with further testing, risk of future dementia. These findings require replication in other well-powered healthy and pathological aging samples, and across a longer time period.

**Disclosure statement**

The authors have no actual or potential conflicts of interest.

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Appendix A. Supplementary data

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References


